

Treating brain cancer with heat therapy using a novel noninvasive microwave applicator



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GBM 2-year survival

Current Standard of Care
SEER Registry 2010-2014

21%

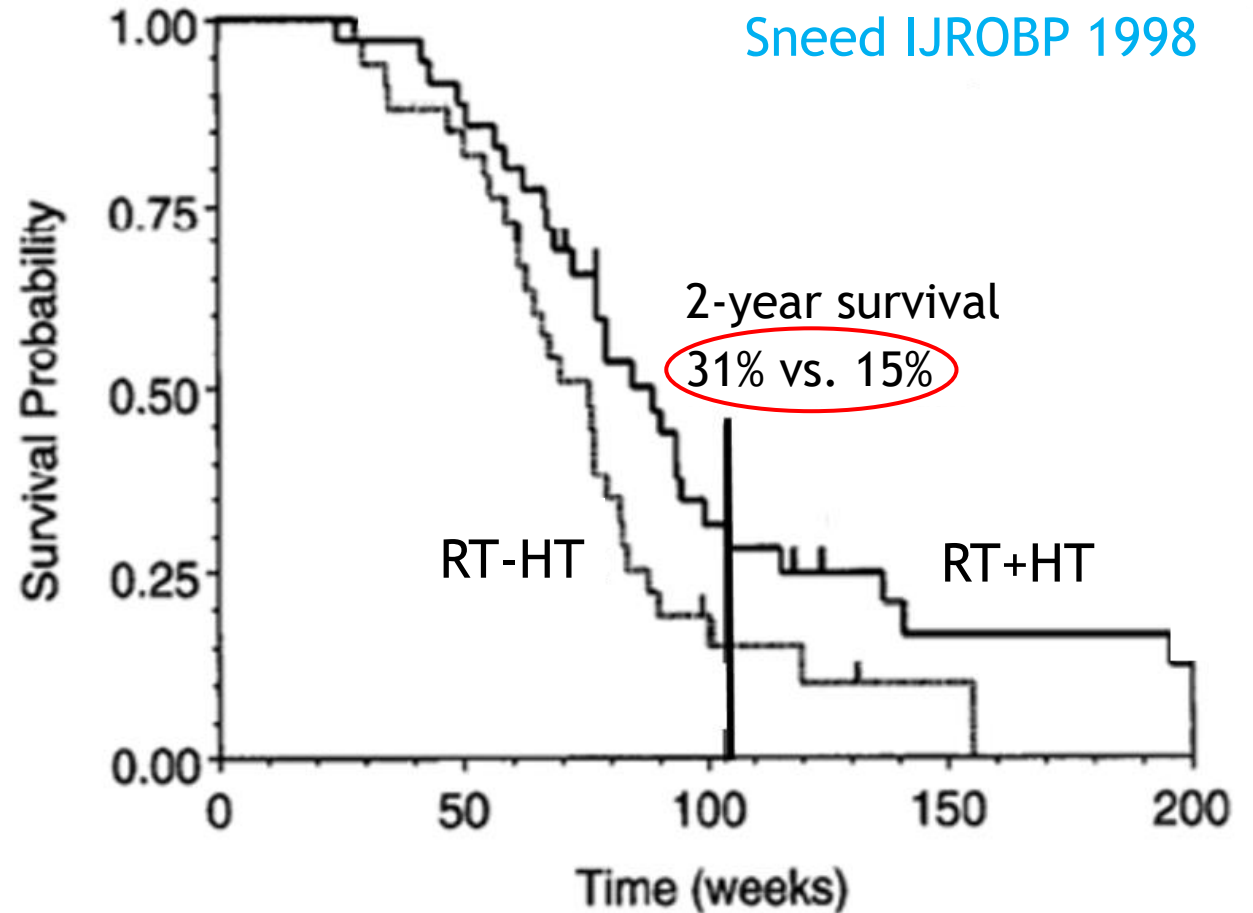


Temozolomide + RT
Stupp et al. 2008, Lancet
(EORTC-NCIC rand phase III)

27%

Randomized Trial in Primary GBM (Conventional RT + brachy boost ± interstitial HT)

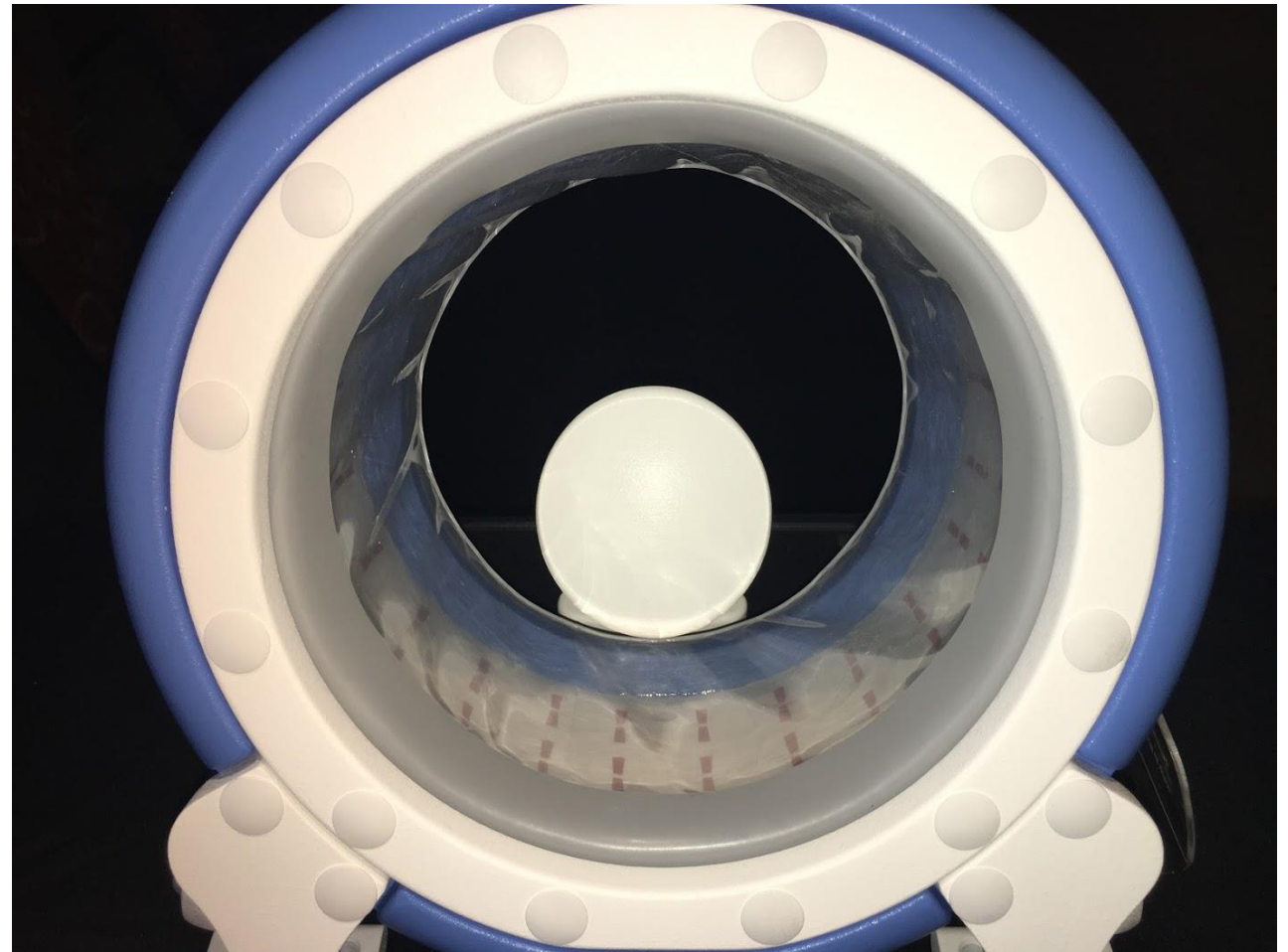
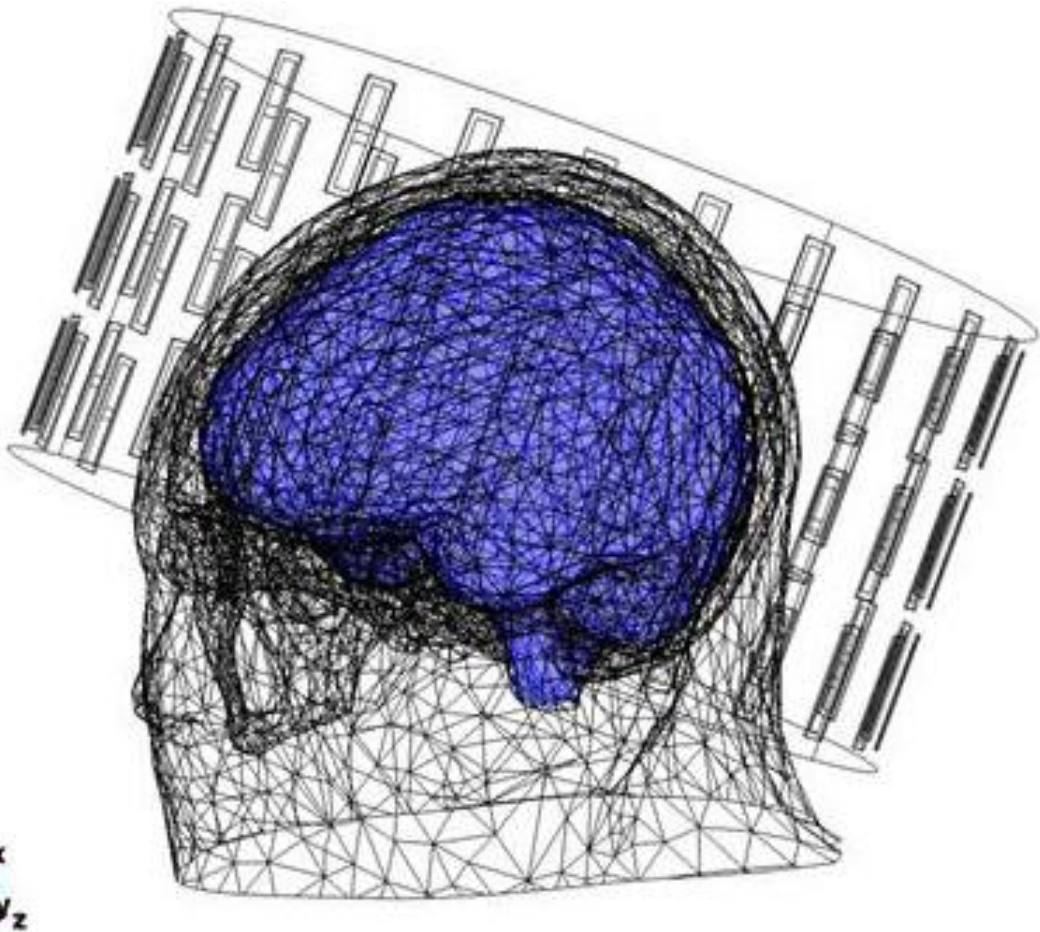
Sneed IJROBP 1998



HT (40-45 °C) doubled 2-year survival!

Noninvasive applicator configuration

- Operating frequency: 915 MHz
- Array: 3 rings of 24 antennas (dipole size 9×24 mm)
- Cylindrical frame: 13 cm length, 26 cm dia. (~4cm water bolus)



Antenna port parametrization

- Fully parametrized port phase and input power for all 72 antennas using 72, 24, or 8 amplifier controls

Global Definitions

- Parameters 1 - controls
- Parameters 2 - model
- Parameters 3 - tests
- Formulas
 - theta, start 7.5deg (*th*)
 - DistanceToTarget N=24 (*Ri*)
 - DistanceToTarget OuterRingN=24 (*Re*)
 - Psi center ring = Psi_i (*PSI*)**
 - Psi outer rings = Psi_e (*PSE*)
 - psi0 8AMP (*psi0*)
 - Psi1_8to24AMP (*psi1*)
 - Psi2_8to24AMP (*psi2*)
 - Relative power (*Pr*)
 - Pr per AMP (*w*)
- Common Model Inputs

Label: Psi center ring = Psi_i

Function name: PSI

Definition

Expression: $(2 * \pi / \lambda_{\text{brain}}) * (R_i(n) - R_{\text{min}})$

Arguments: n

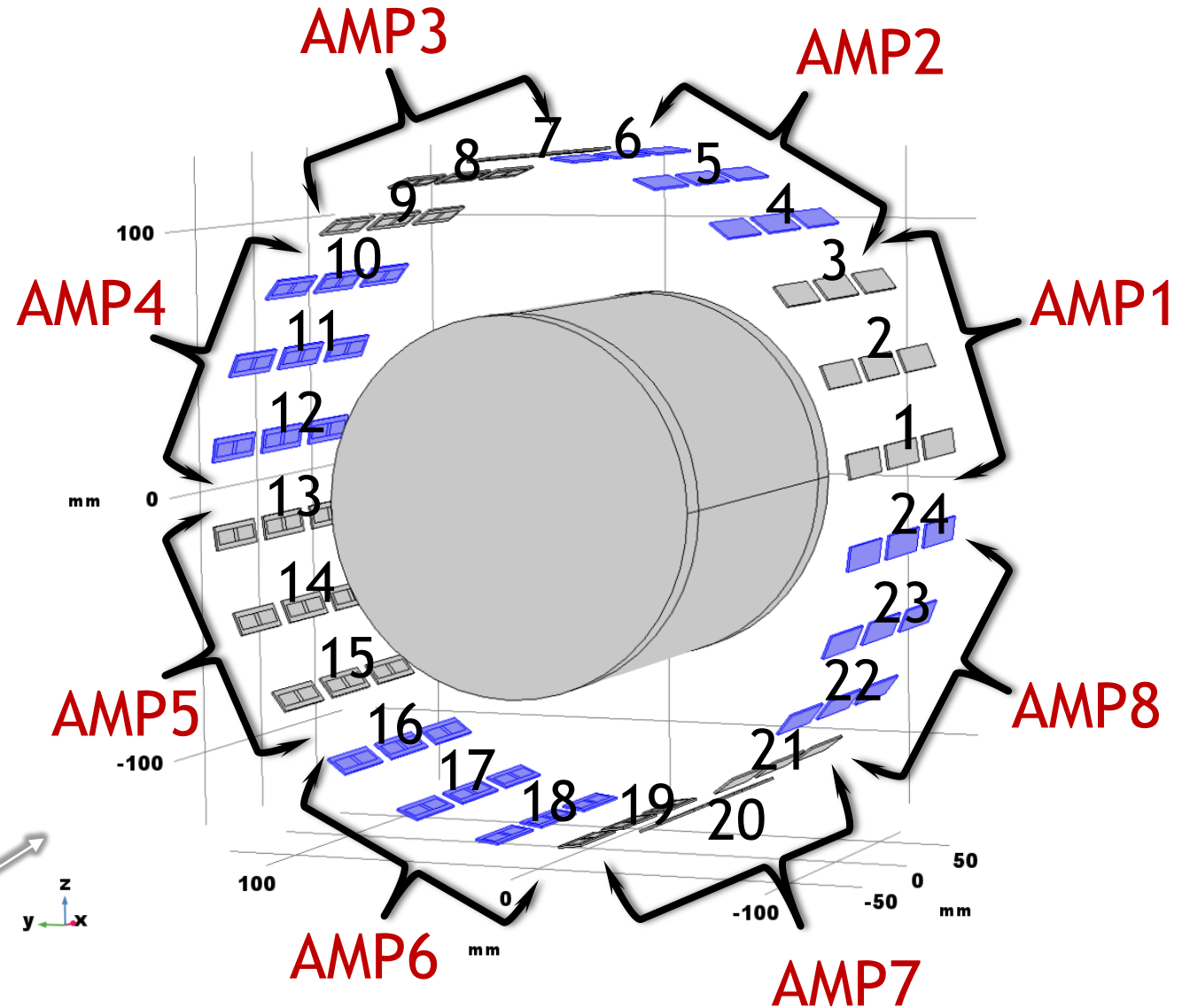
Derivatives: Automatic

Periodic Extension

Units

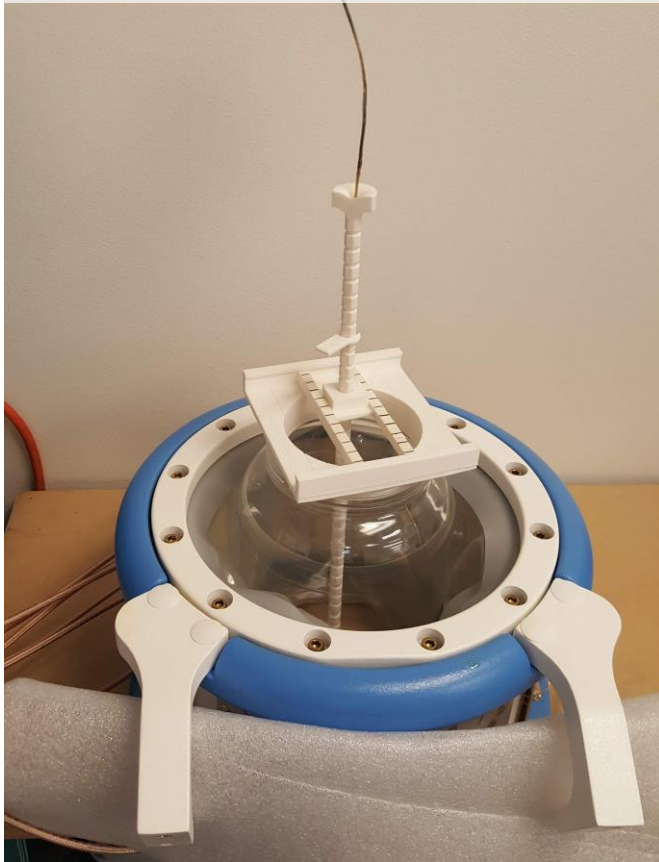
Arguments:

Function: rad



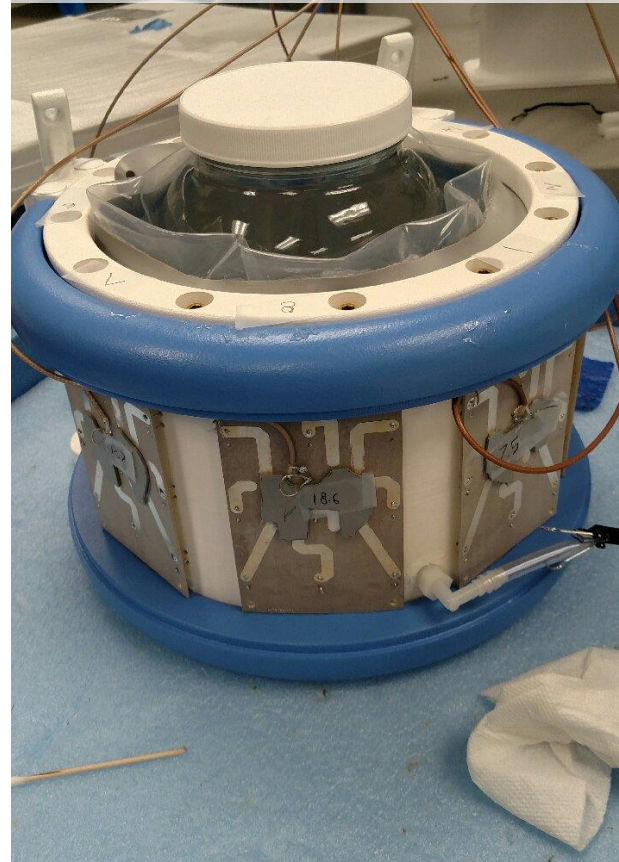
Practical applicator design involves using 8 amplifiers controlling 9 antennas each

Setup for E-field measurements



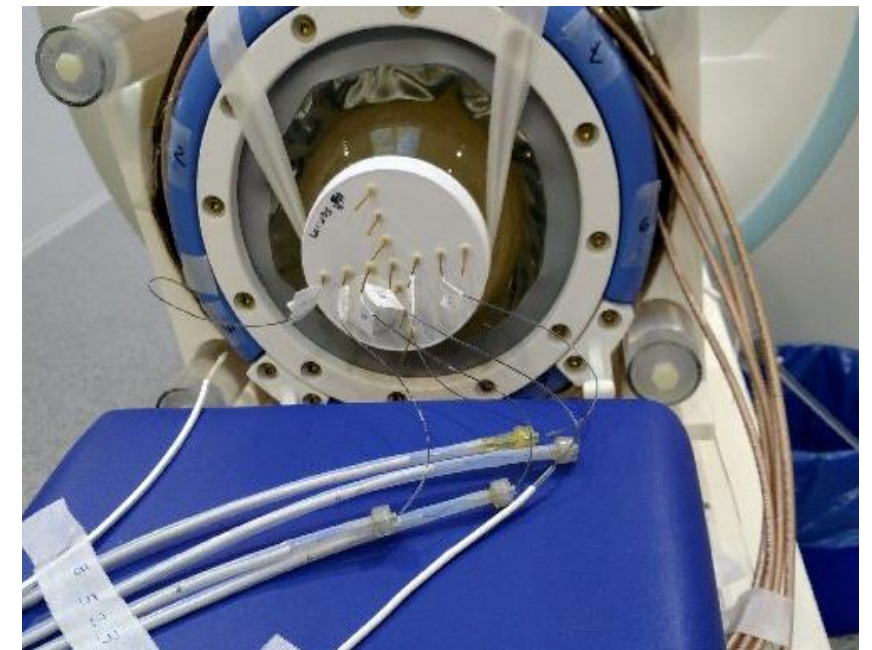
E-field sensor - miniature dipole 12mm long

Phantom Heating measurements



BSD-500 915MHz
8 channel generator

Setup for Thermometry 3D MR, SigmaVision Advanced & 1D RF-insensitive thermistors

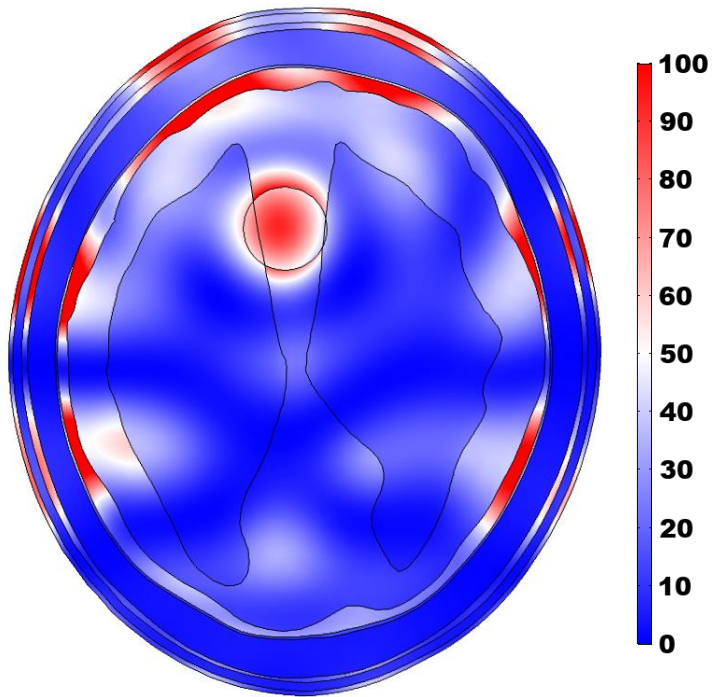


1.5T MRI system
(Magnetom Symphony)

Computational modeling methods: RF→HT↔FF

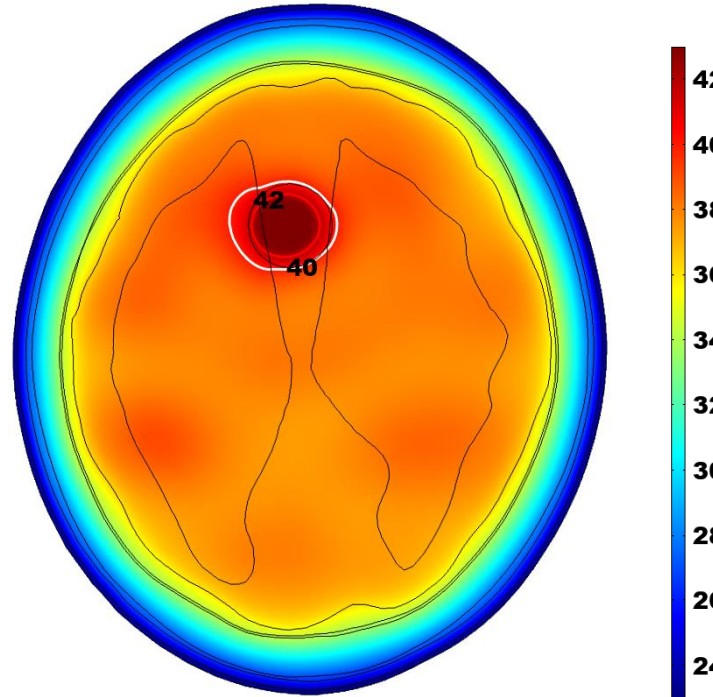
RF
Module

Specific absorption rate, SAR (%)



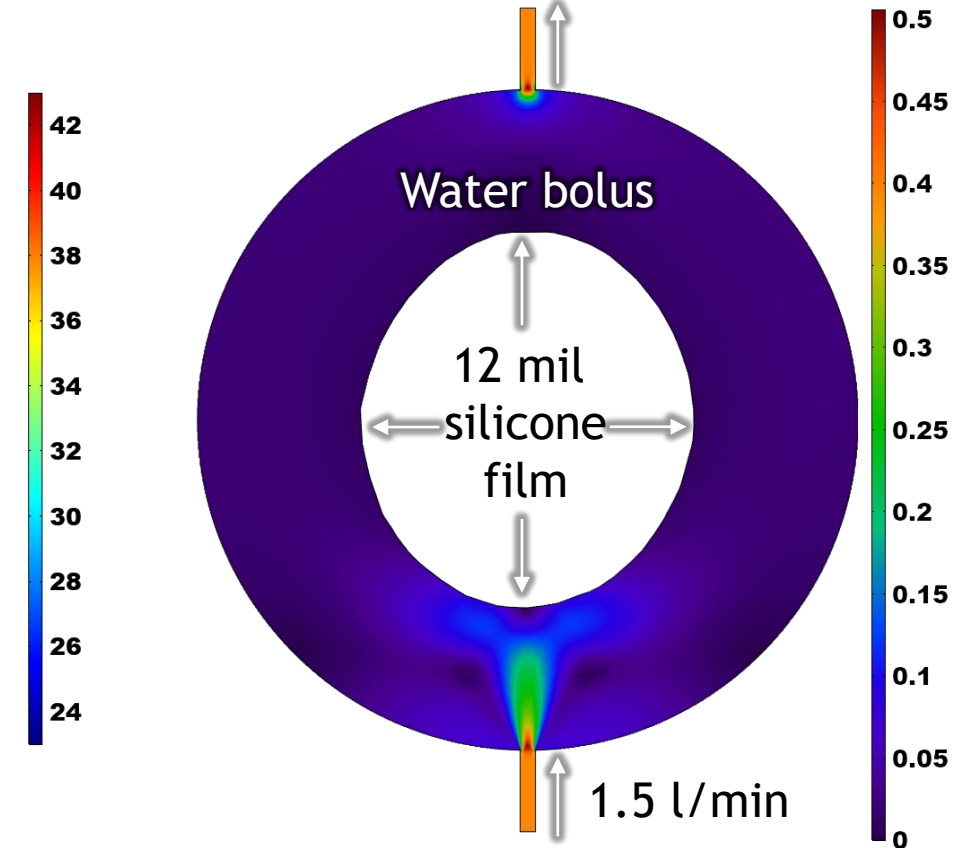
Heat Transfer
Module

Temperature (°C)



CFD
Module

Velocity (cm/s)



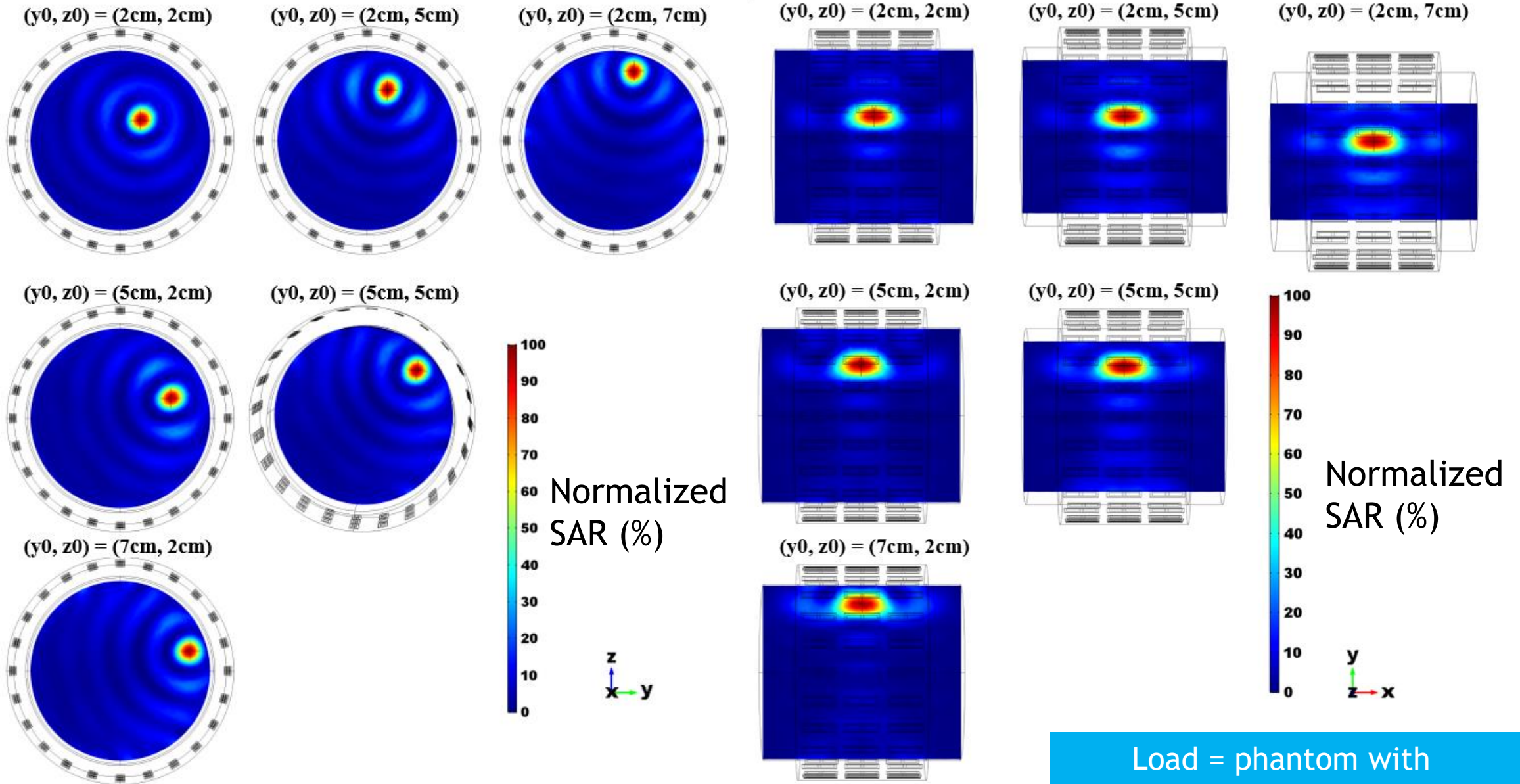
CAD Import
Module

Material
Library

Optimization
Module

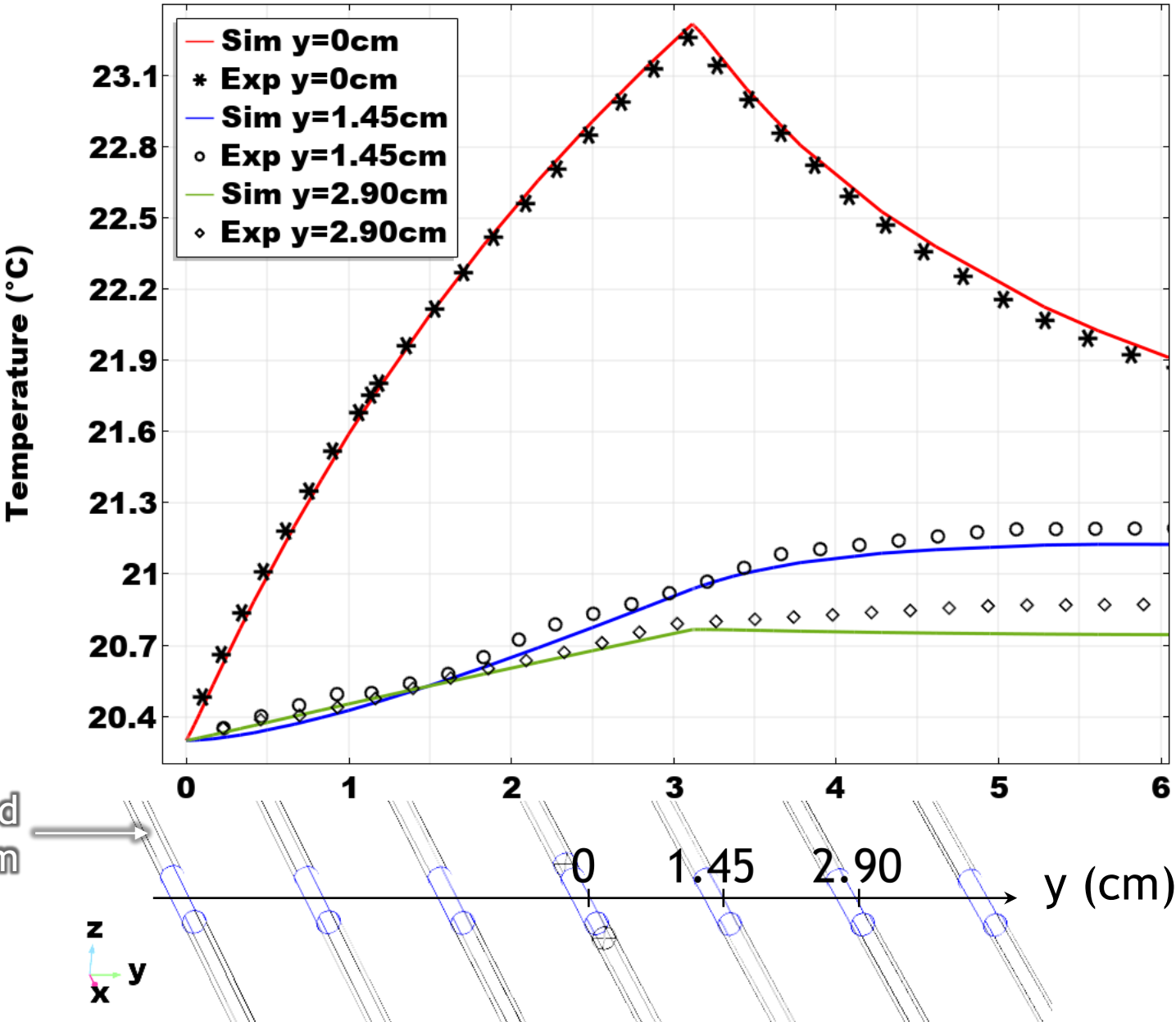
Fluid flow embedded in a boundary condition in HT
using average $h_{\text{bolus}} = 50 \text{ W/m}^2/\text{K}$ and $T_{\text{bolus}} = 23^\circ\text{C}$

Steering with 72 amplifiers in a phantom



Load = phantom with
18 cm diameter \times 20 cm length

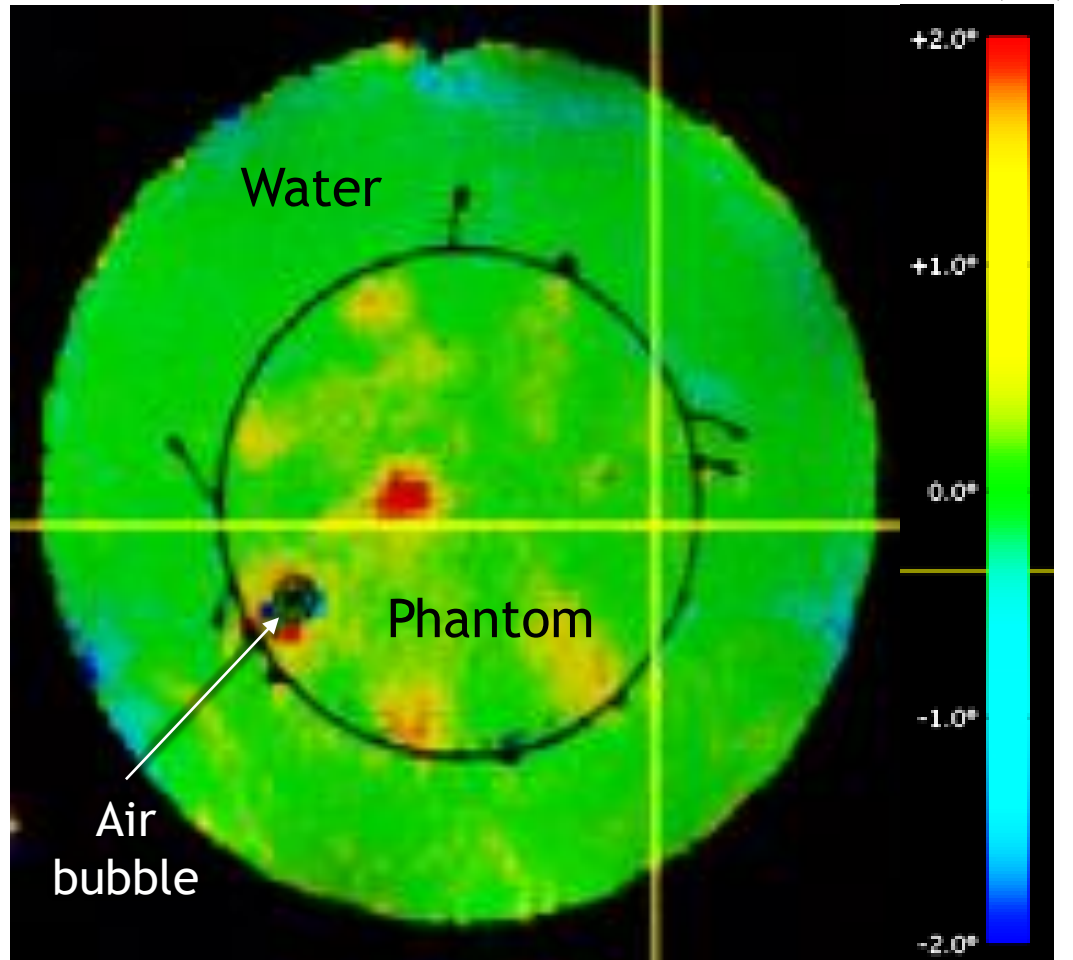
Simulation vs Experimental probe thermometry



Target = phantom center
(0,0,0) cm

Simulation vs Experimental MR thermometry

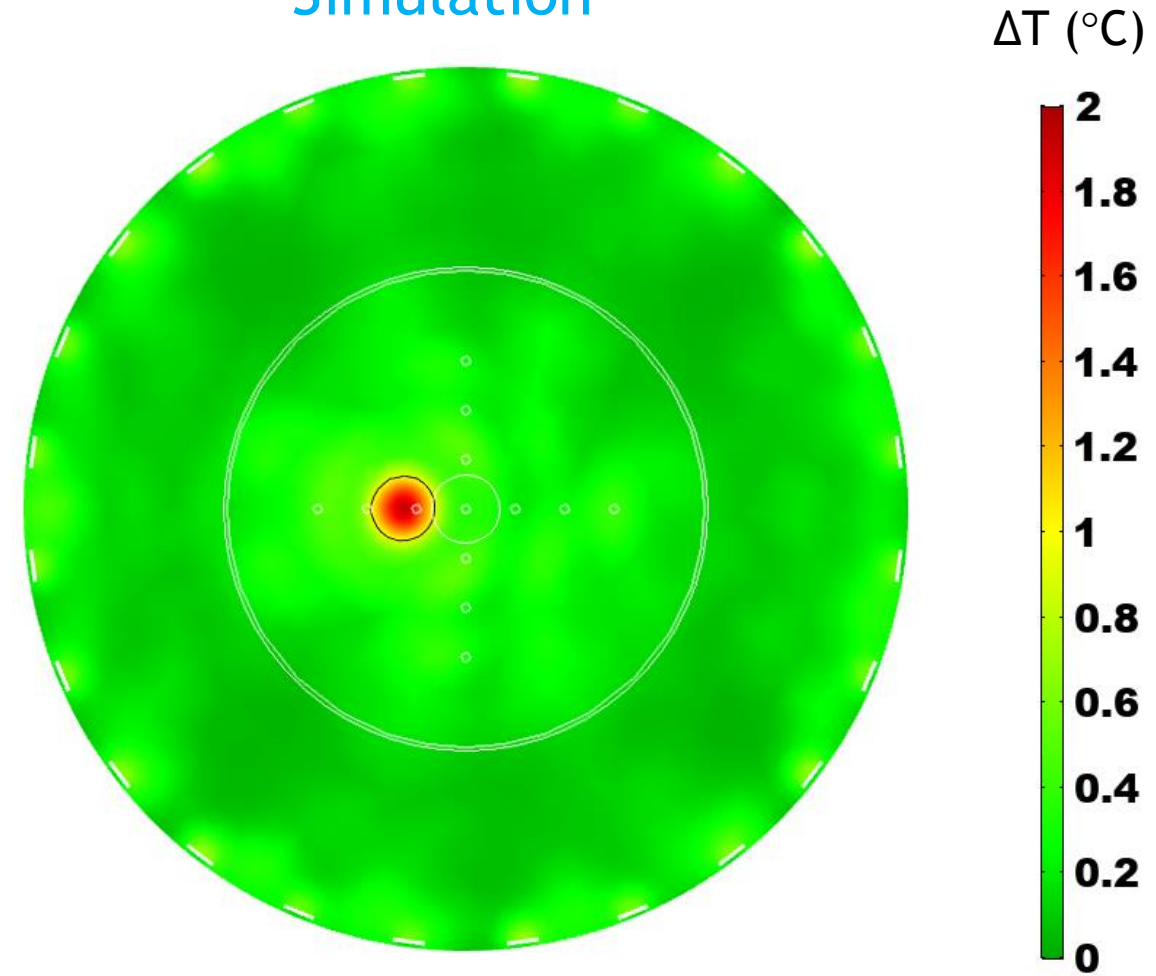
MR scan (experimental)



$\Delta y = 16$ mm
Heat focus = $4 \times 1.5 \times 1.5$ cm³

$$\text{Heat focus} = \frac{\Delta T_{\text{max}}}{2}$$

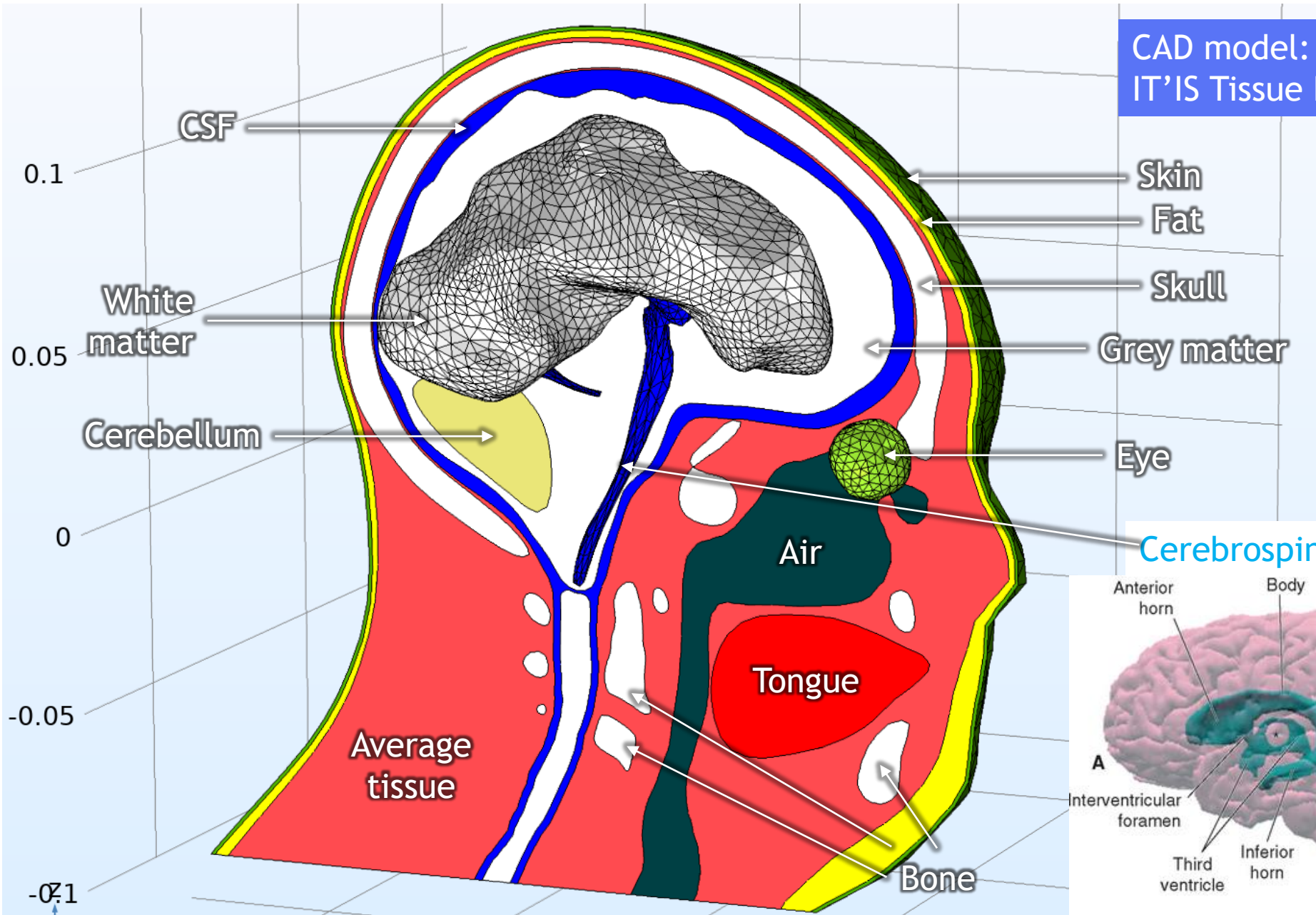
Simulation



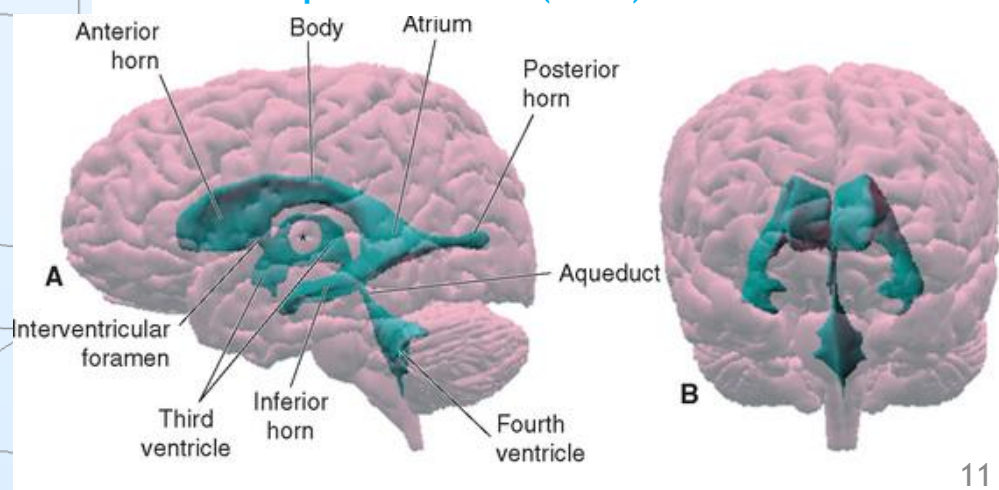
$\Delta y = 18$ mm
Heat focus = $3.4 \times 1.4 \times 1.5$ cm³

Anatomical model

CAD model: Neva Electromagnetics v3.0
IT'IS Tissue Property database v4.0



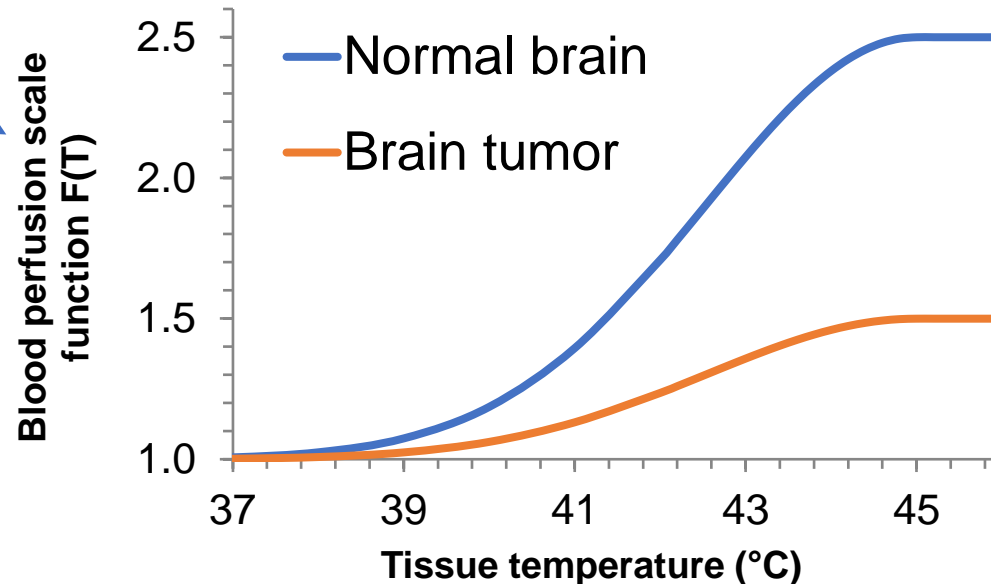
Cerebrospinal fluid (CSF) ventricles



- Power optimized based on $T_{\text{tumor}} = 40\text{-}44^\circ\text{C}$, $T_{\text{normal}} < 42^\circ\text{C}$
- Necrotic core (2 cm) with 10% of white matter blood perfusion
- Water bolus convective cooling: $T_{\text{bolus}} = 23^\circ\text{C}$, $h_{\text{bolus}} = 50 \text{ W/m}^2/\text{K}$
- Bioheat equation with temperature dependent blood perfusion:

$$\omega_B(T) = \omega_b \times F(T)$$

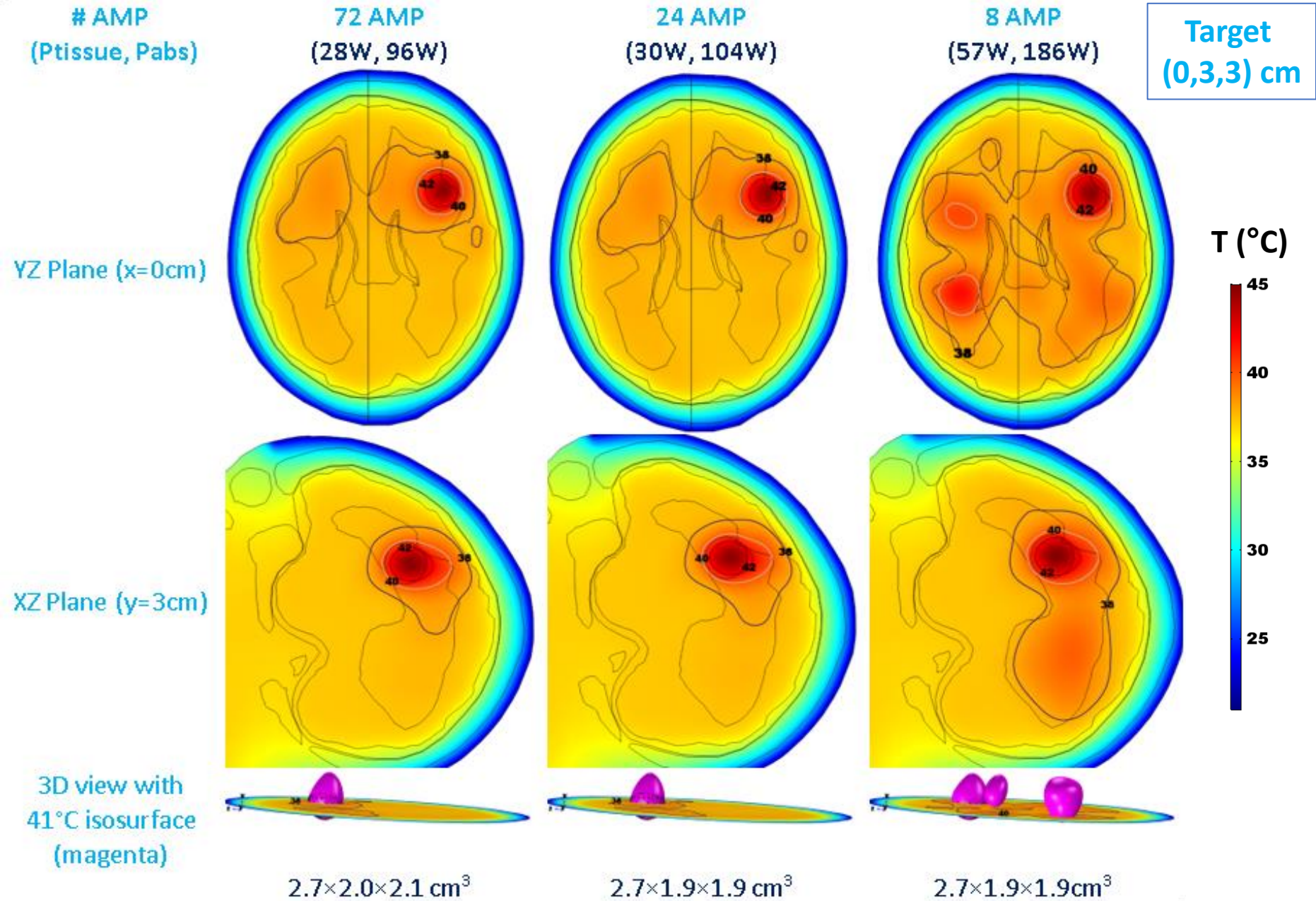
Basal blood perfusion



2, EM+FF+HT
Optimization
Step 1: Time Dependent
Solver Configurations

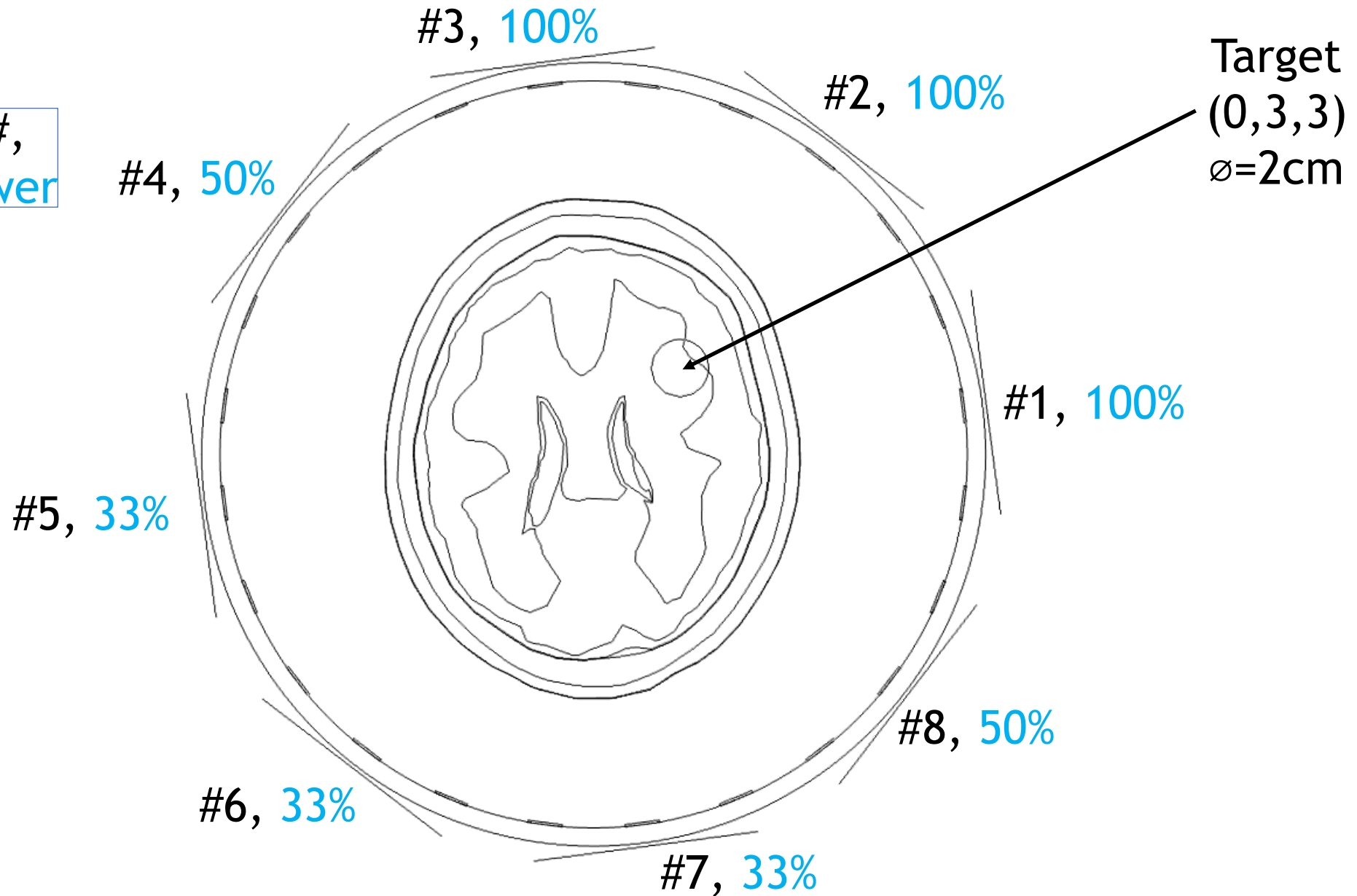
Component 1 (comp 1)
Definitions
Variables
Interpolation 1 (wn)
Interpolation 2 (wt)

Steering with 72→8 amplifiers



Relative power optimization 1 / 2

Amplifier #,
Relative power

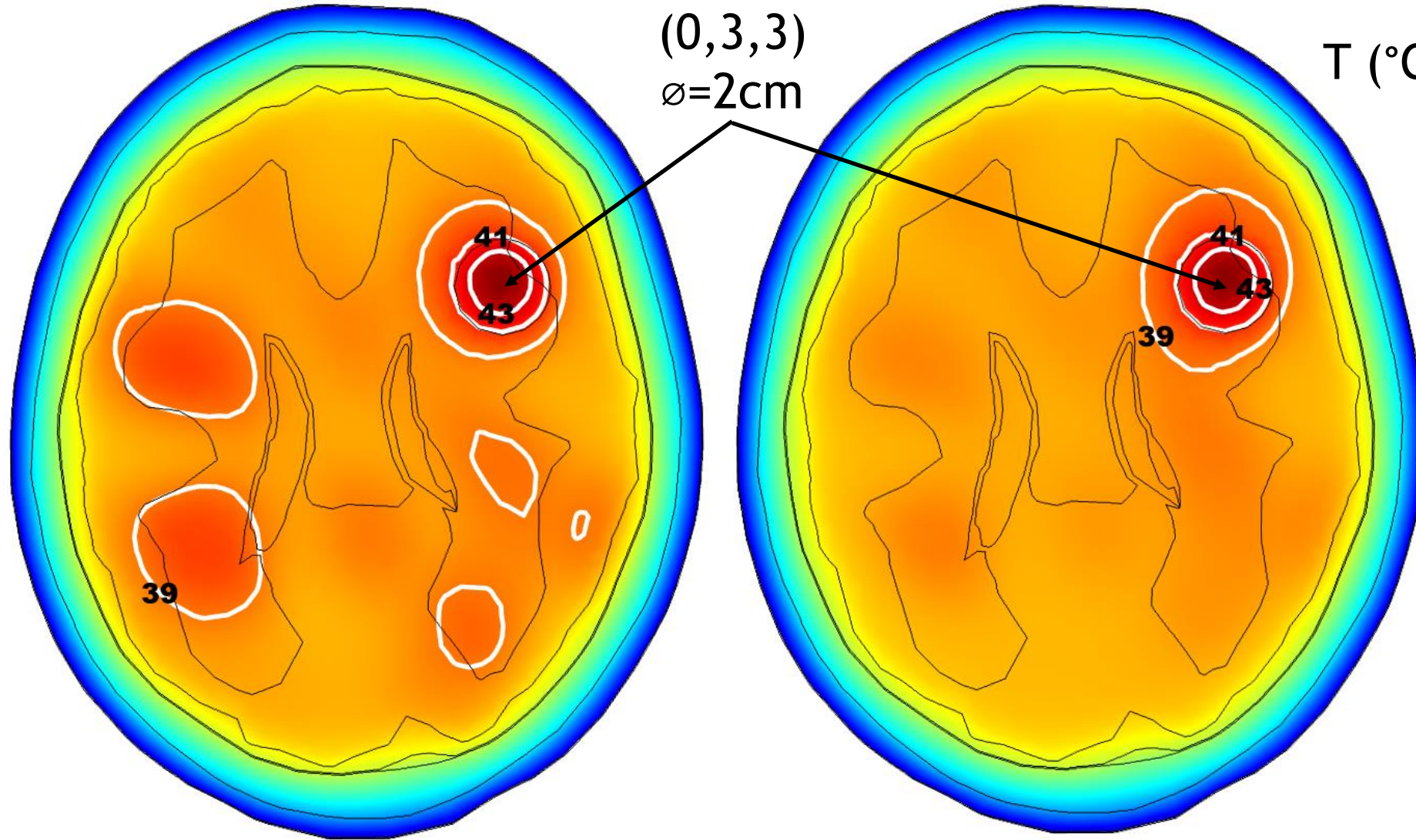
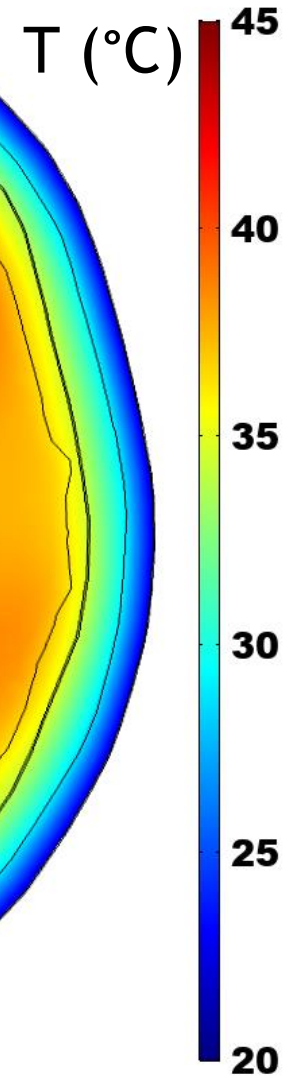


Relative power optimization 2/2

Before

After relative power
optimization

Target
(0,3,3)
 $\varnothing=2\text{cm}$



- 3D MR and 1D thermometry validated COMSOL numerical simulations
- The feasibility of heating small targets in a head phantom using a novel microwave brain applicator is demonstrated with experiments and numerical simulations
- Phantoms confirm reliable and predictable focus steering
- 8 channels may have phase control limitations, but using improves thermal dose in target while reducing hot spots in healthy tissue
- By providing a dedicated noninvasive HT brain applicator, focused heating will likely significantly increase clinical outcomes of GBM cancer treatments using radiation and/or chemotherapy, as it has in many other clinical trials that used adjuvant HT